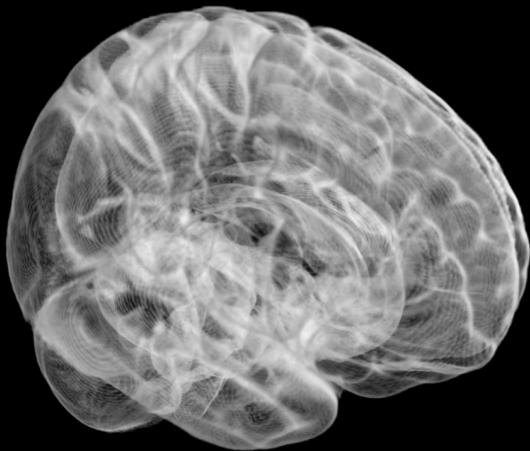


# Machine learning for brain imaging

Gaël Varoquaux

INRIA/Parietal

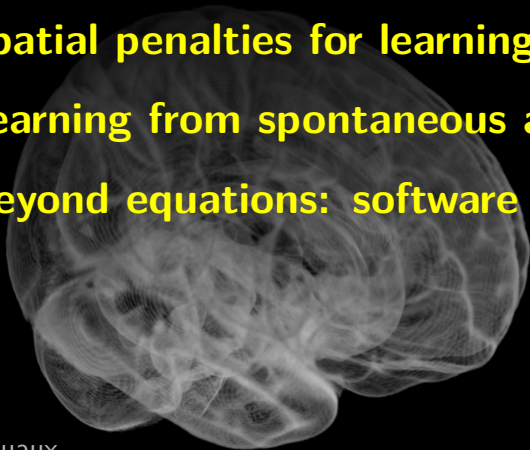


 PARIETAL

*Inria*

NeuroSpin

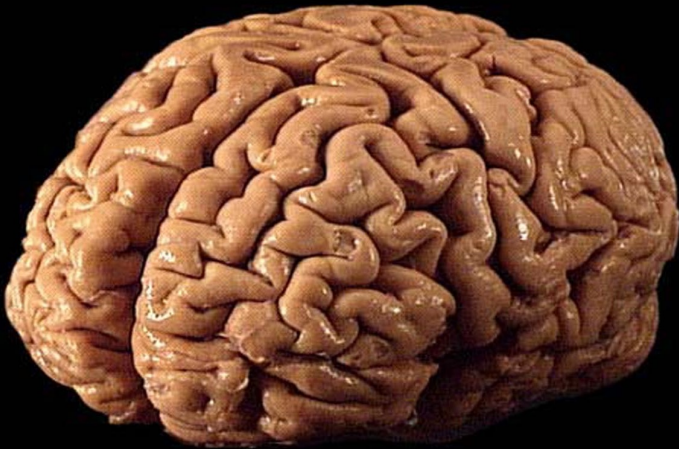
- 1 An introduction to brain imaging**
- 2 Learning to diagnose**
- 3 Understanding brain function**
- 4 Spatial penalties for learning from images**
- 5 Learning from spontaneous activity**
- 6 Beyond equations: software**



# 1 An introduction to brain imaging

- The brain: its anatomy and function
- Imaging the brain

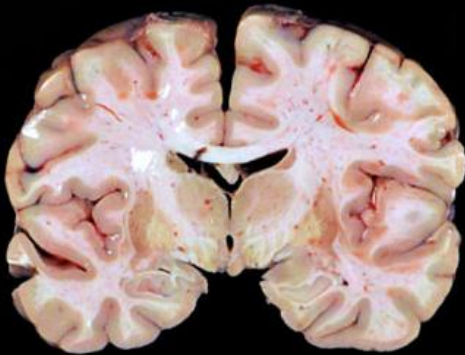
# The brain: its anatomy and function



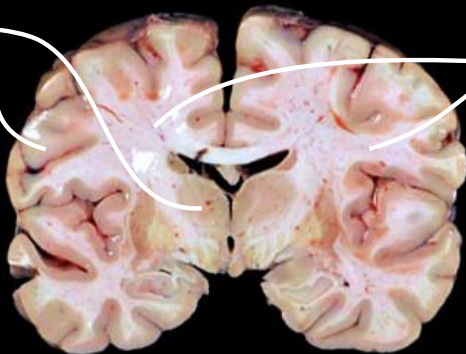
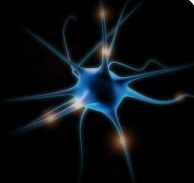
■ Two hemispheres

■ “sulci”

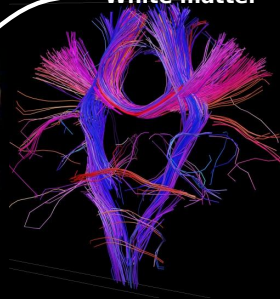
# 1 Inside a brain: neuroanatomy in one minute



Grey matter



White matter



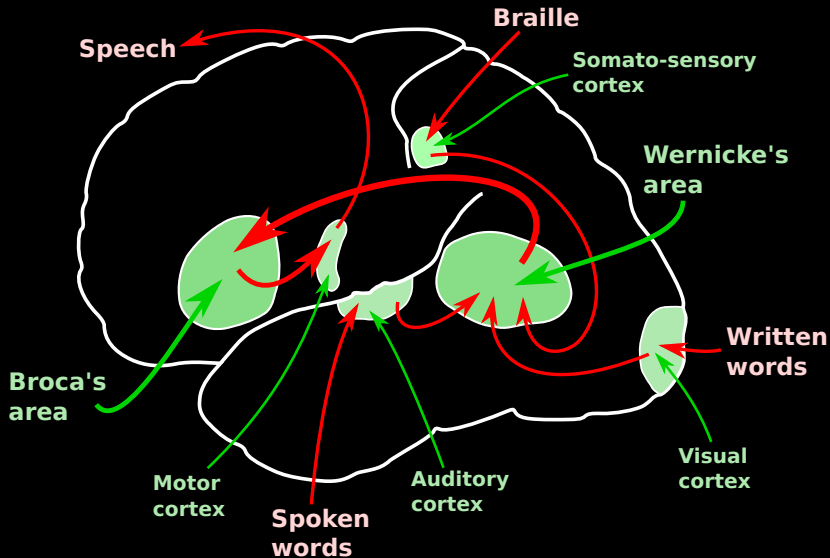
Grey matter

White matter

Cortex

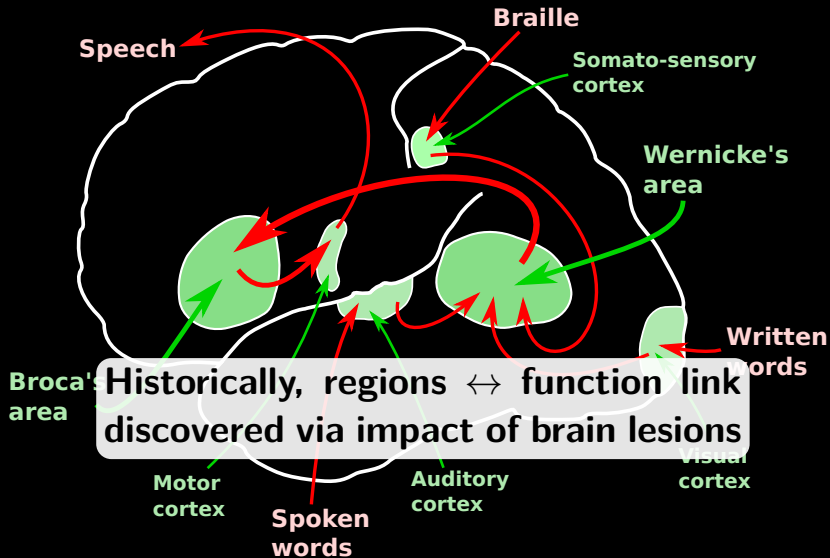


### The language circuit:

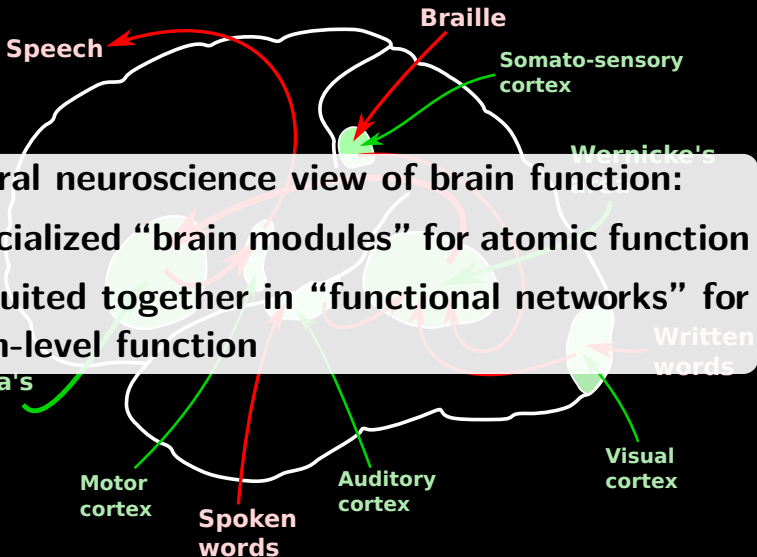




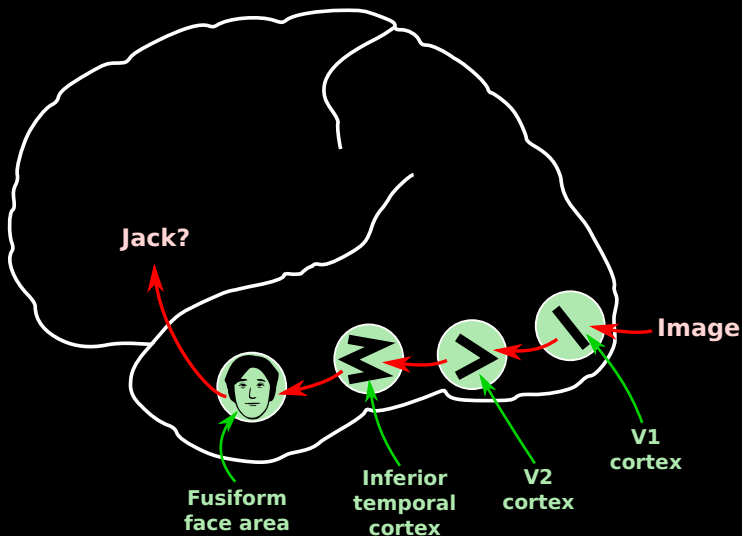
## The language circuit:



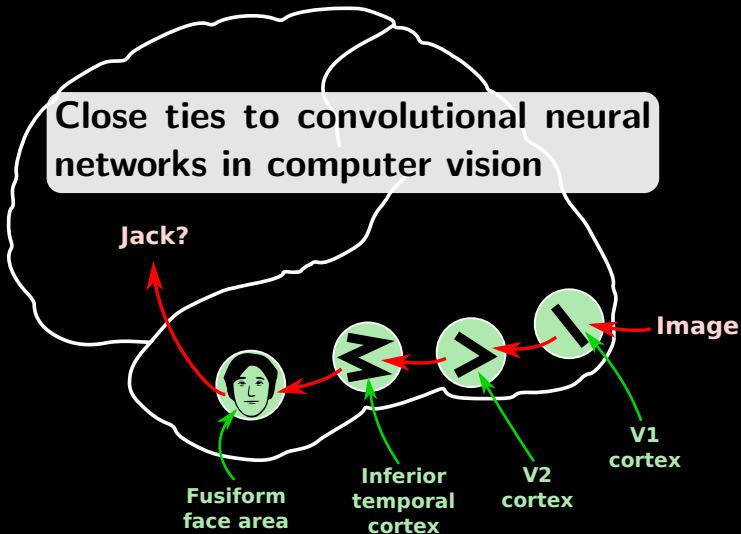
## The language circuit:



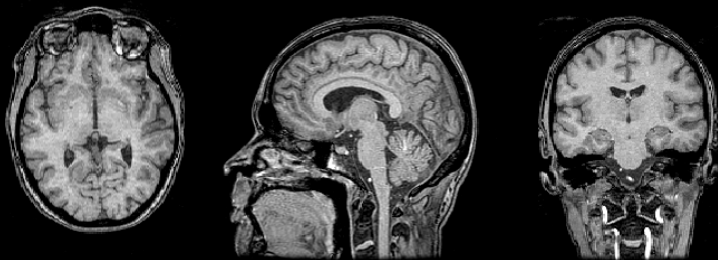
## The visual system: a computational model



## The visual system: a computational model



## Imaging the brain



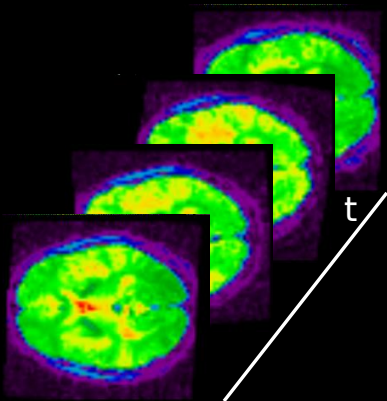
3D images

# 1 anatomical MRI

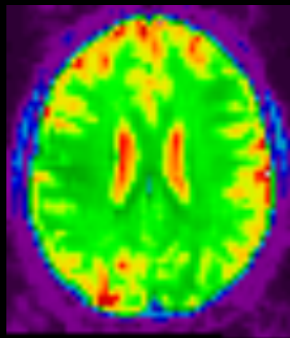


- White matter, grey matter
- Cortex

# 1 functional MRI (fMRI)



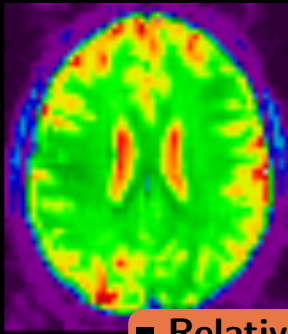
Time-resolved recordings of brain activity



## Blood Oxygen Level Dependent effect

- MRI probes local magnetic properties
- oxyHemoglobin and deoxyHemoglobin have different magnetic susceptibility
- Neural activity consumes oxygen
  - ⇒ Initial dip in oxyHemoglobin
- Metabolism compensates
  - ⇒ Increase in oxyHemoglobin





## Blood Oxygen Level Dependent effect

- MRI probes local magnetic properties
- oxyHemoglobin and deoxyHemoglobin have different

■ Neural

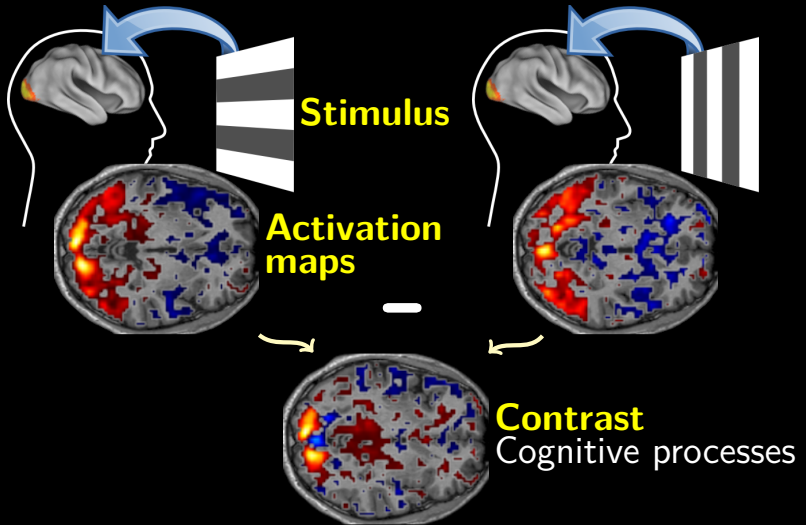


■ Metab

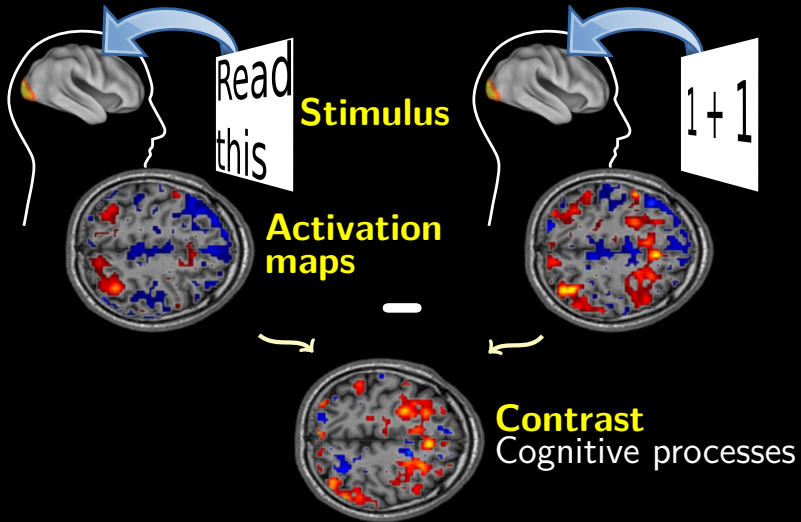


- Relative effect, not absolute  
⇒ Need to contrast values
- Very indirect effect  
⇒ Non-linearities, inhomogeneities, lags...  
All models are wrong

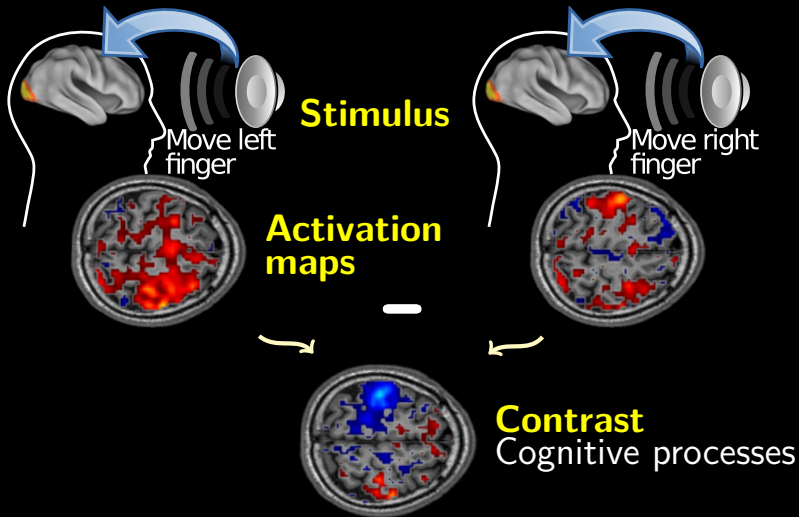
# 1 Mapping cognition with fMRI



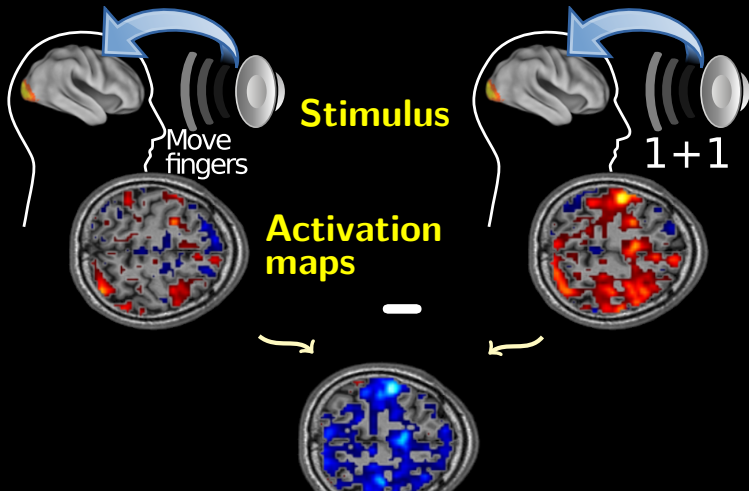
# 1 Mapping cognition with fMRI



# 1 Mapping cognition with fMRI



# 1 Mapping cognition with fMRI



Careful crafting of contrasts to isolate high-level cognition

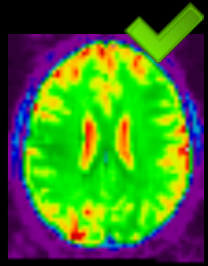
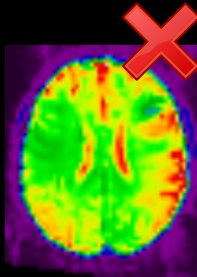
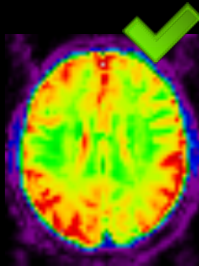
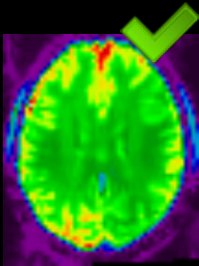
# 1 Magneto and electro encephalography

- Measure electromagnetic field created by neural fixing
- “Interesting” inverse problem to reconstruct sources on cortex
  - ⇒ Poor spatial resolution
- Great temporal resolution

## 2 Learning to diagnose



# Diagnostic applications: promises and challenges





## 2 Diagnosis, prognosis, and biomarkers

### Diagnosis

Finding the nature or cause of a disease condition

### Pronosis

Predicting the future evolution of the condition

⇒ Therapeutic indications

### Early biomarkers

Measures enabling the detection of disease before standard symptoms

⇒ Population screening if cheap

### Quantitative biomarkers

Metric to follow disease progression

⇒ Drug development

## 2 Specificity – sensitivity trade-offs

Depending on application, different types of error may need to be weighted differently

*E.g.:* Screening before human check

Low false negative rate, high false positive rate

Detection leading to surgery

Low false positive rate

## 2 More than prediction accuracy

Cannot replace the physician:

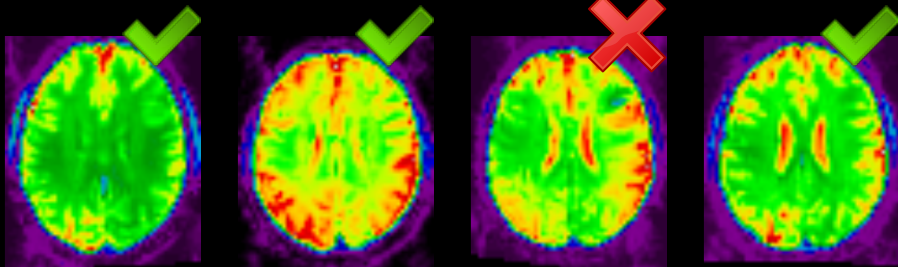
- Patient history
- Therapeutic strategies subject to logistics

...

⇒ No black-box

Segmentation, denoising task

as much as prediction



## 2 More than prediction accuracy

Cannot replace the physician:

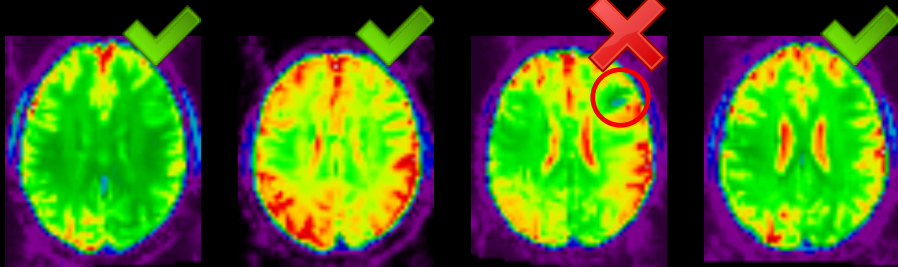
- Patient history
- Therapeutic strategies subject to logistics

...

⇒ No black-box

Segmentation, denoising task

as much as prediction



## 2 The training set is not representative

- Early or weakly-symptomatic patients not represented  
these are the most interesting
- Label noise: wrong diagnostic on difficult patients  
⇒ validation difficult
- Confounding factors for patients  
  
⇒ Epidemiological studies (biobank, UK)  
select subjects randomly from  
normal population, and follow them  
  
but imaging cost prohibitive

## 2 The training set is not representative

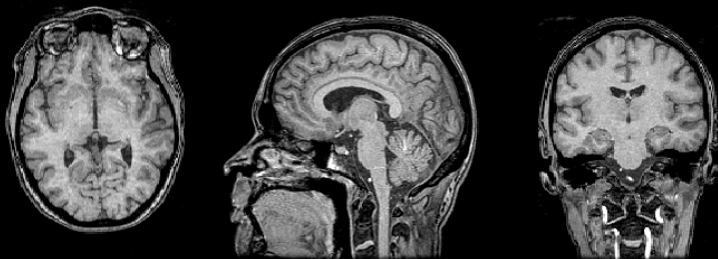
- Early or weakly-symptomatic patients not represented  
these are the most interesting
- Label noise: wrong diagnostic on difficult patients  
⇒ validation difficult
- Confounding factors for patients

**Real problems are not patient/control classifications, but multi-pathology classifications**

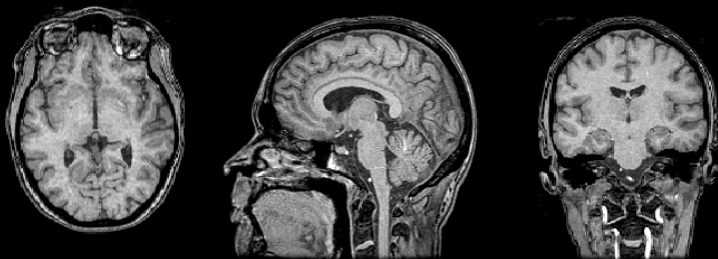
**Datasets are small (not many subjects)**

- Researchers don't share data
- Large inter-site variability

## Features from brain images



## Features from brain images

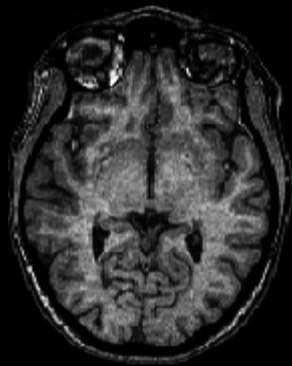


Not a standard computer vision pipeline!

- Brains are not translation-invariant
- We don't understand much about the brain  
but we still know *something*



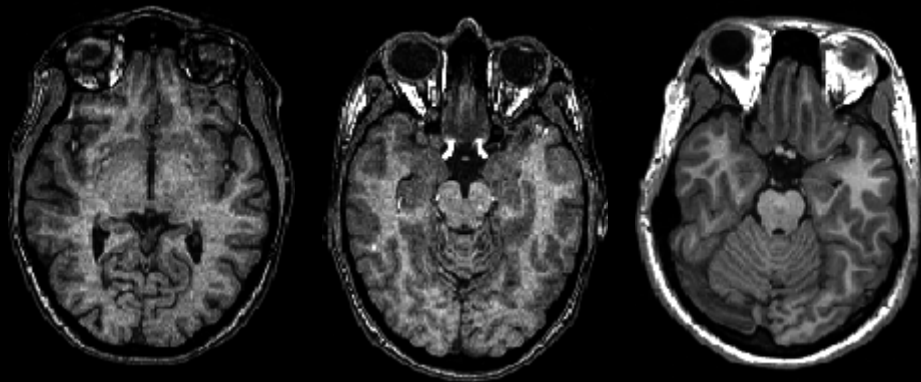
## 2 Features in anatomical images



### What are we trying to capture?

- Changes in brain shape?
- Local grey-matter changes?
- Micro-lesions?

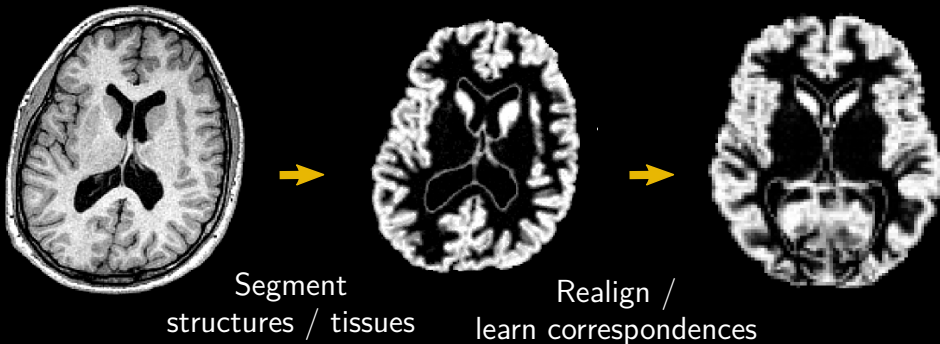
## 2 Features in anatomical images



- Changes in brain shape?
- Local grey-matter changes?
- Micro-lesions?

**Across subjects**

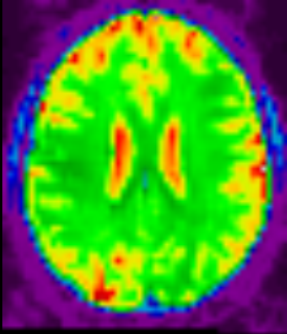
## 2 Feature extraction in anatomical images



### Features in structures or in correspondence vectors

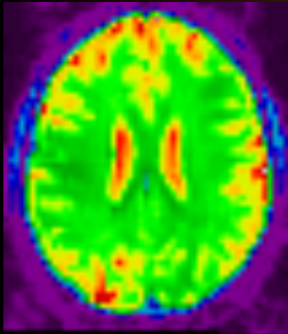
- Voxel-based morphometry: grey matter density
- Cortical thickness
- Shape descriptors of cortex
- Realignment transformation field

## 2 Functional images



**Functional images are low SNR**  
Why use them?

## 2 Functional images



**Functional images are low SNR**

Why use them?

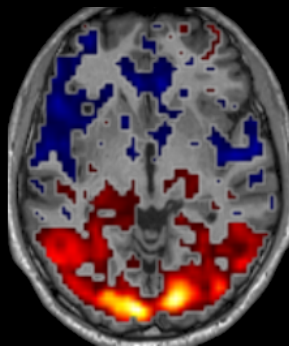
- Behavioral deficit vary for a given lesion
- Neuro-psychiatric diseases (autism, schizophrenia) = deficit of function with no known anatomy



**Des troubles  
de la parole**

## 2 Features in functional images

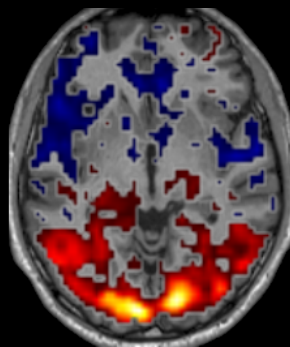
### Activation maps to dissect cognitive effects



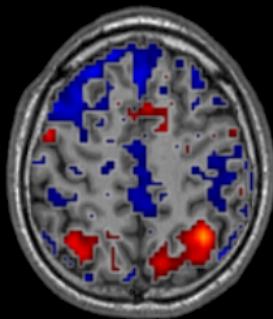
Images

## 2 Features in functional images

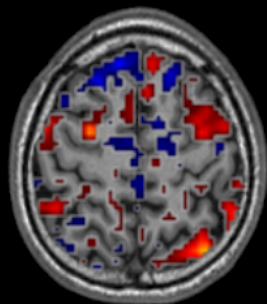
### Activation maps to dissect cognitive effects



Images



Reading



Counting

Often: one map per stimuli presentation

[Poldrack 2011]

# 3 Understanding brain function

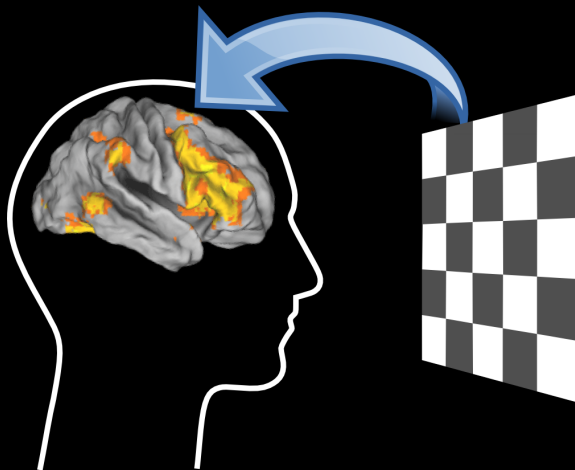
## Cognitive neuroimaging





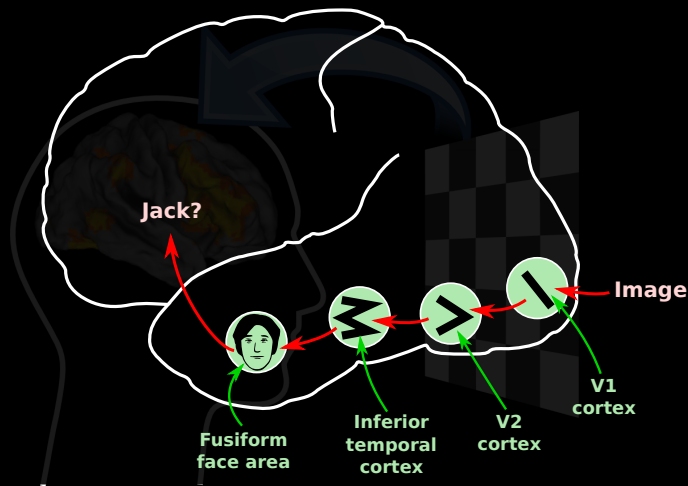


### 3 Machine learning for cognitive neuroImaging



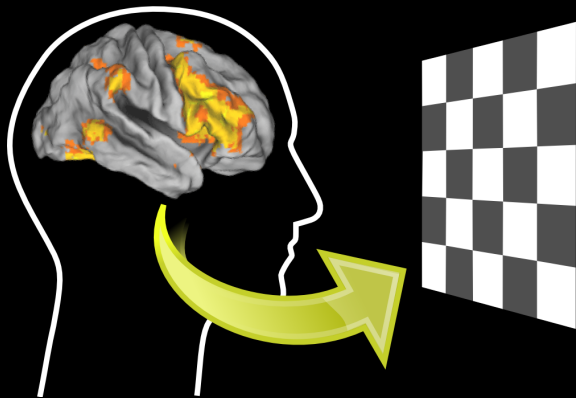
**Predicting neural response:**  
encoding models

### 3 Machine learning for cognitive neuroImaging



**Predicting neural response:**  
encoding models

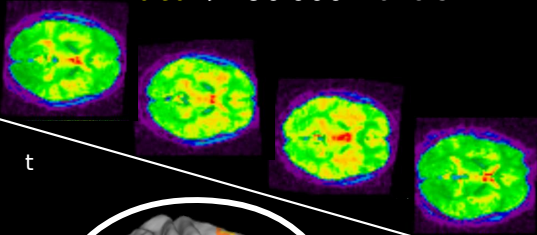
### 3 Machine learning for cognitive neuroImaging



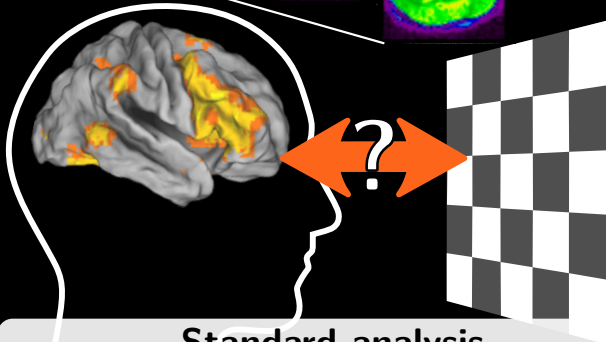
***“Brain reading”***: decoding

### 3 Brain mapping

fMRI data > 50 000 voxels



stimuli



**Standard analysis**

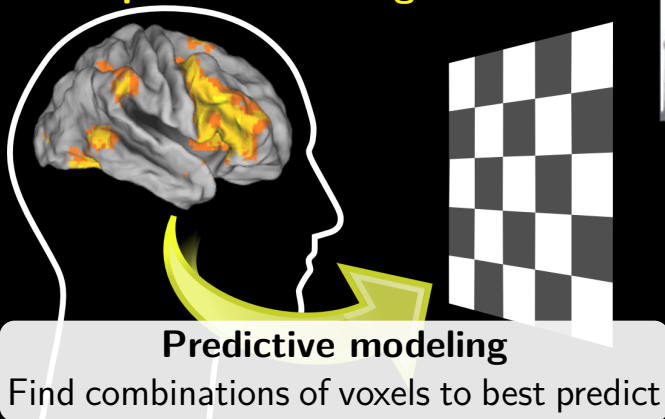
Detect voxels that correlate to the stimuli

### 3 Brain mapping $\Leftrightarrow$ brain reading

#### ■ Predicting the object category viewed

[Haxby 2001, *Distributed and Overlapping Representations of Faces and Objects in Ventral Temporal Cortex*]

#### Supervised learning task



### 3 Brain mapping $\Leftrightarrow$ brain reading

#### ■ Predicting the object category viewed

[Haxby 2001, *Distributed and Overlapping Representations of Faces and Objects in Ventral Temporal Cortex*]

**Take home message:  
brain regions, not prediction**

**Face area**



**Place area**

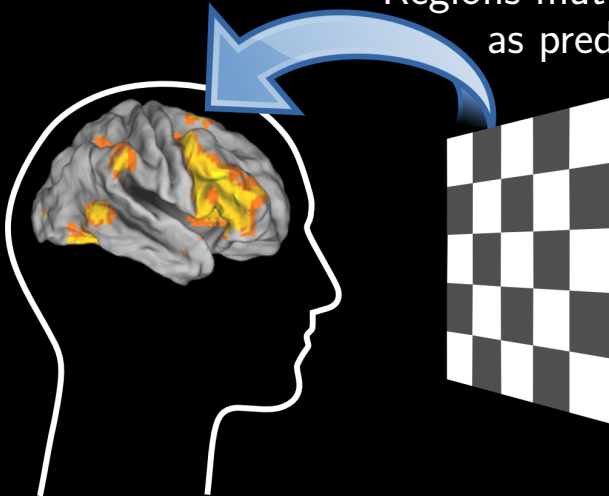
**Predictive modeling**

Find combinations of voxels to best predict



## Recovery rather than prediction

Regions matter as much  
as prediction score



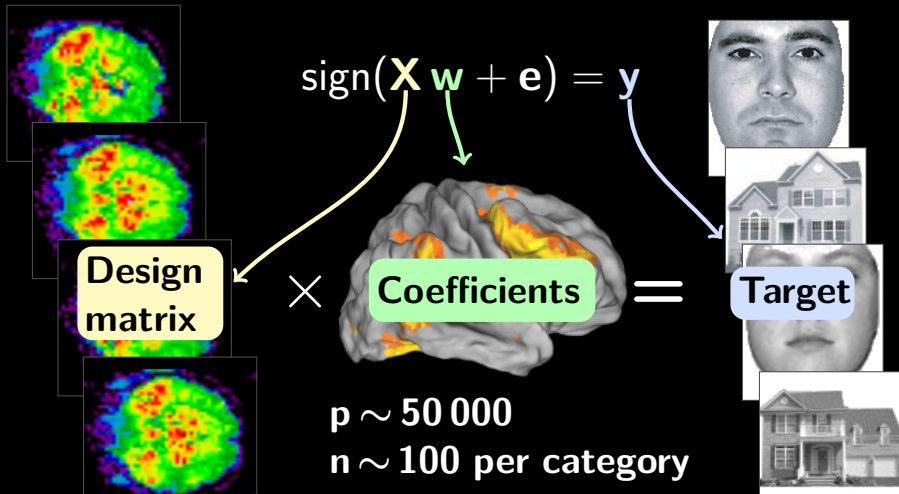


## Recovery rather than prediction

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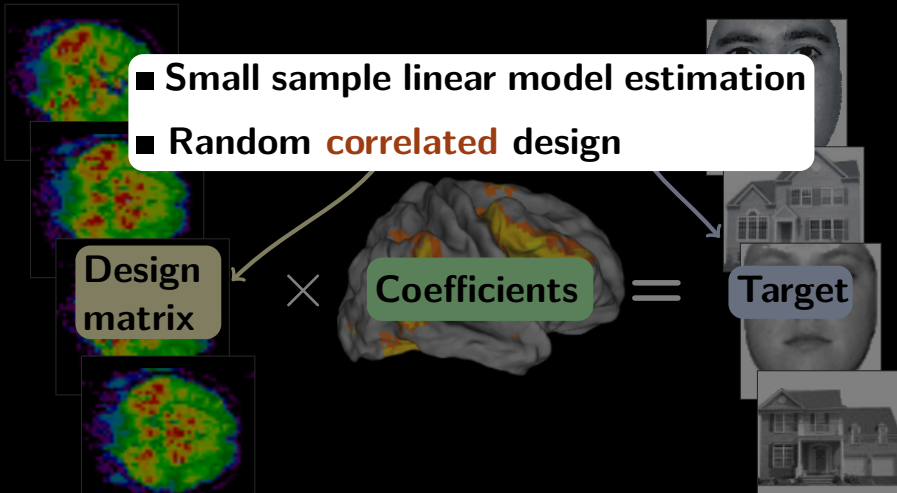


## 4 Spatial penalties for learning from images



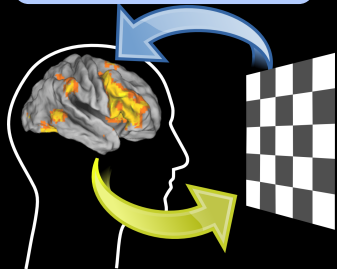
## 4 Spatial penalties for learning from images

- Small sample linear model estimation
- Random **correlated** design



## 4 Estimation: statistical learning

### Inverse problem



- Minimize an error term:

$$\hat{\mathbf{w}} = \underset{\mathbf{w}}{\operatorname{argmin}} l(\mathbf{y} - \mathbf{X} \mathbf{w})$$

Ill-posed:  $\mathbf{X}$  is not full rank

- Inject prior: regularize

$$\hat{\mathbf{w}} = \underset{\mathbf{w}}{\operatorname{argmin}} l(\mathbf{y} - \mathbf{X} \mathbf{w}) + p(\mathbf{w})$$

## 4 Estimation: statistical learning

Inverse problem

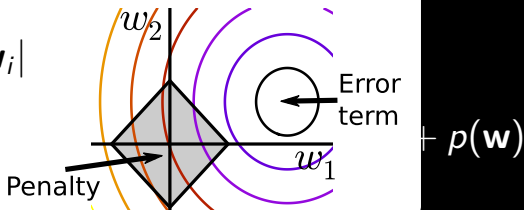
■ Minimize an error term:

$$\hat{\mathbf{w}} = \underset{\mathbf{w}}{\operatorname{argmin}} \ell(\mathbf{y} - \mathbf{X} \mathbf{w})$$

Example: Lasso = sparse regression

$$\hat{\mathbf{w}} = \underset{\mathbf{w}}{\operatorname{argmin}} \|\mathbf{y} - \mathbf{X} \mathbf{w}\|_2^2 + \ell_1(\mathbf{w})$$

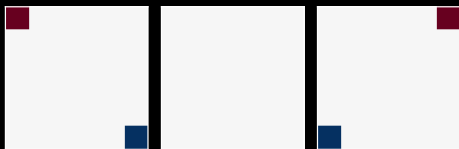
$$\ell_1(\mathbf{w}) = \sum_i |\mathbf{w}_i|$$



## 4 Good prediction $\neq$ good recovery

### Simulations

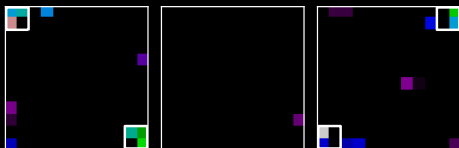
Ground truth



### Lasso

Prediction: 0.78

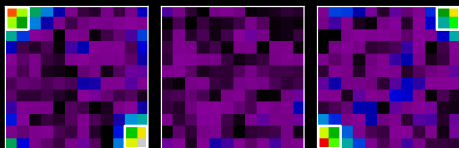
Recovery: 0.429



### SVM

Prediction: 0.71

Recovery: 0.486



**Need a method suited for recovery**

## 4 Brain mapping & $\ell_1$ sparse recovery

Recovering brain regions



## 4 Brain mapping & $\ell_1$ sparse recovery

Recovering  $k$  non-zero coefficients

■  $n_{\min} \sim 2 k \log p$

■ Restricted-isometry-like property:

The design matrix is well-conditioned  
on sub-matrices of size  $> k$

[Candes 2006]

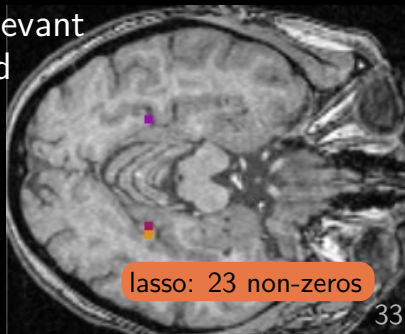
[Tropp 2004]

[Wainwright 2009]

■ Mutual incoherence:

Relevant features  $S$  and irrelevant  
ones  $\bar{S}$  are not too correlated

**Violated by spatial  
correlations in our design**





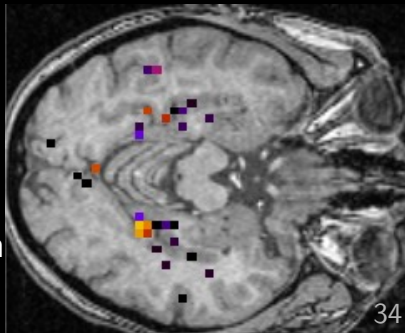
## 4 Randomized sparsity

[Meinshausen and Buhlmann 2010, Bach 2008]

- Perturb the design matrix:
  - Subsample the data
  - Randomly rescale features
- + Run sparse estimator
- Keep features that are often selected
  - ⇒ **Good recovery without mutual incoherence**
  - But RIP-like condition

**Cannot recover large correlated groups** 😞

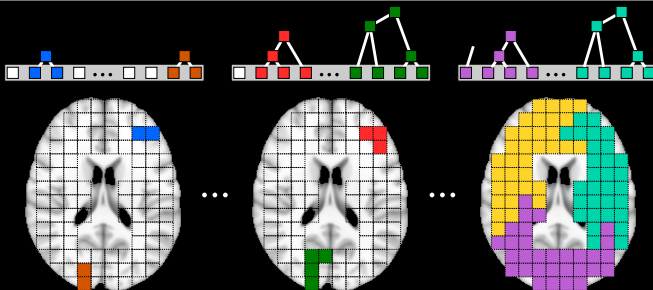
For  $m$  correlated features,  
selection frequency divided by  $m$



## 4 Brain parcellations

### Spatially-connected hierarchical clustering

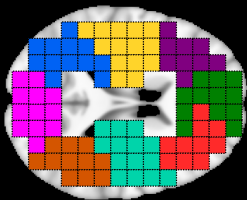
⇒ reduces voxel numbers [Michel Pat Rec 2011]



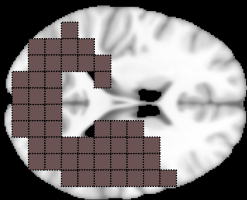
- Replace features by corresponding cluster average
- + Use a supervised learner on reduced problem

☹️ **Cluster choice sub-optimal for regression** ☹️

# 1<sup>st</sup> approach: randomized clustering



Combining  
Clustering

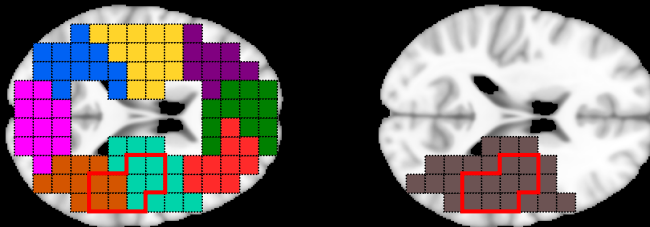


Sparsity

[Varoquaux ICML 2012]

## 4 Brain parcellations + sparsity

**Hypothesis:** clustering compatible with support( $\mathbf{w}$ )

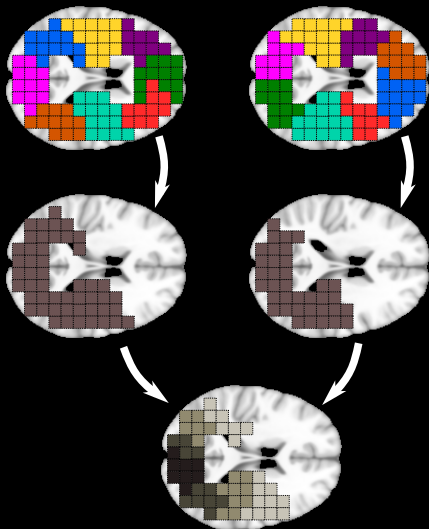


### Benefits of clustering

- Reduced  $k$  and  $p$ 
  - $\Rightarrow n > n_{\min}$ : good side of the “sharp threshold”
- Cluster together correlated features
  - $\Rightarrow$  Improves RIP-like conditions

Recovery possible on reduced features

## 4 Randomized parcellations + sparsity



### Randomization + Stability scores

- ■ ■
- Marginalize the cluster choice
- ■ ■
- Relaxes mutual incoherence requirement

## 4 Algorithm

1 set `n_clusters` and `sparsity` by cross-validation

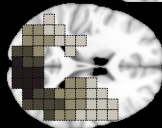
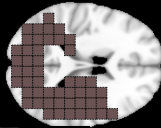
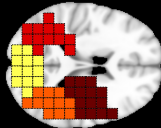
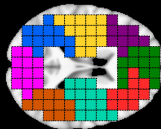
2 loop: perturb randomly data

3 clustering to form reduced features

4 sparse linear model on reduced features

5 accumulate non-zero features

6 threshold map of apparition counts



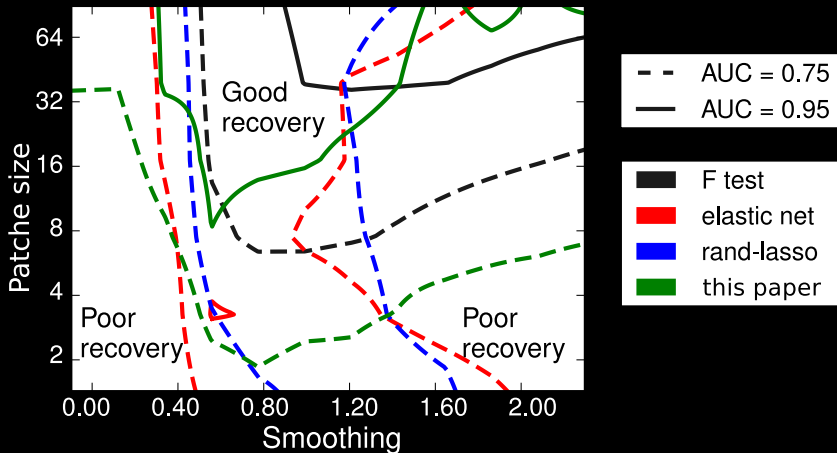
## 4 Simulations

- $p = 2048, k = 64, n = 256$  ( $n_{\min} > 1000$ )
- Weights  $\mathbf{w}$ : patches of varying size
- Design matrix: 2D Gaussian random images of varying smoothness

### Estimators

- Randomized lasso
- Elastic Net
- Our approach
- Univariate F test

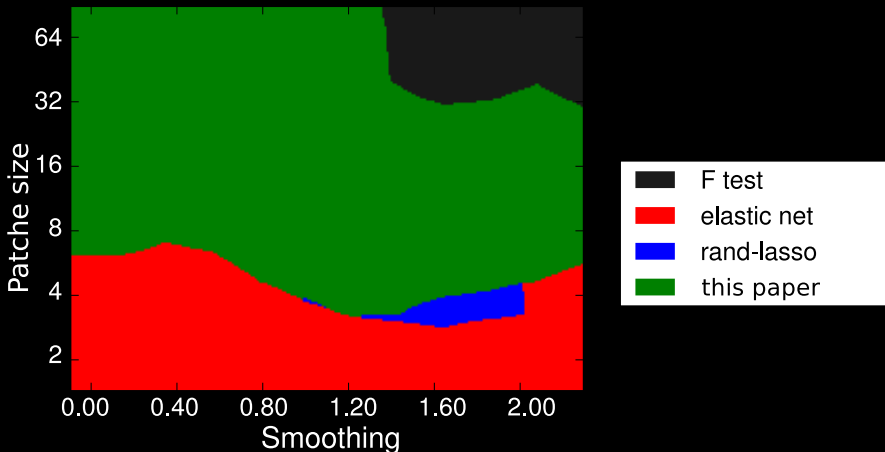
## 4 When can we recover patches?



- Smoothness helps (reduces noise degrees of freedom)
- Small patches are hard to recover

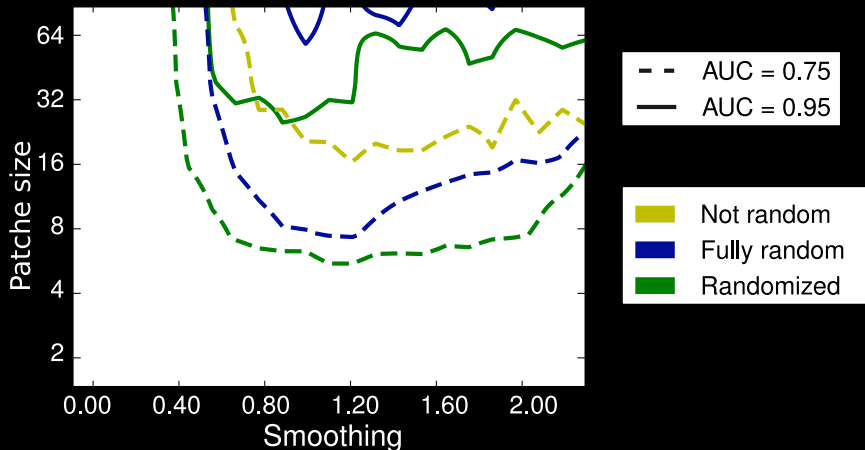


## 4 What is the best method for patch recovery?



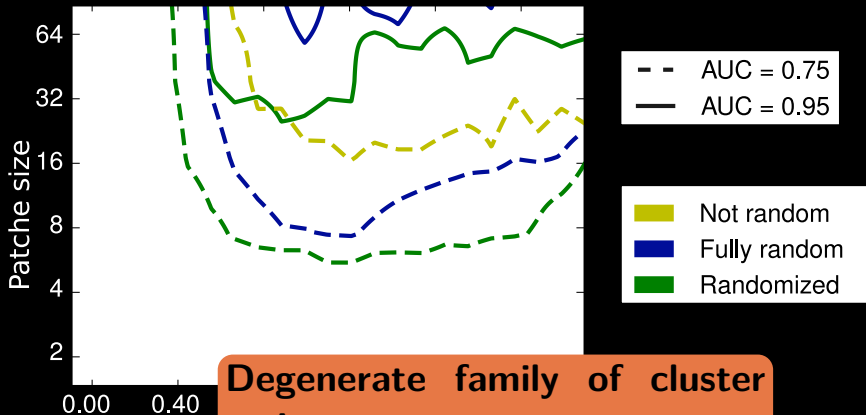
- For small patches: elastic net
- For large patches: randomized-clustered sparsity
- Large patches and very smooth images: F-test

## 4 Randomizing clusters matters!



- Non-random (Ward) clustering inefficient
- Fully-random performs quite well
- Randomized Ward gives an extra gain

## 4 Randomizing clusters matters!

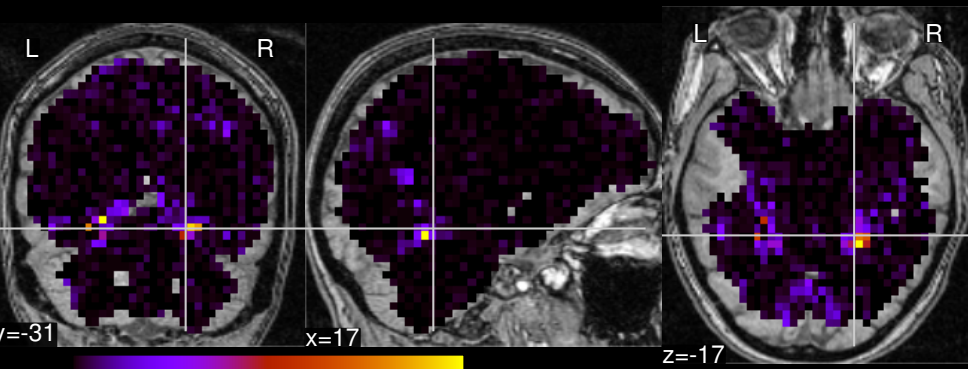


Degenerate family of cluster assignments

- Non-random (Ward) clustering inefficient
- Fully-random performs quite well
- Randomized Ward gives an extra gain

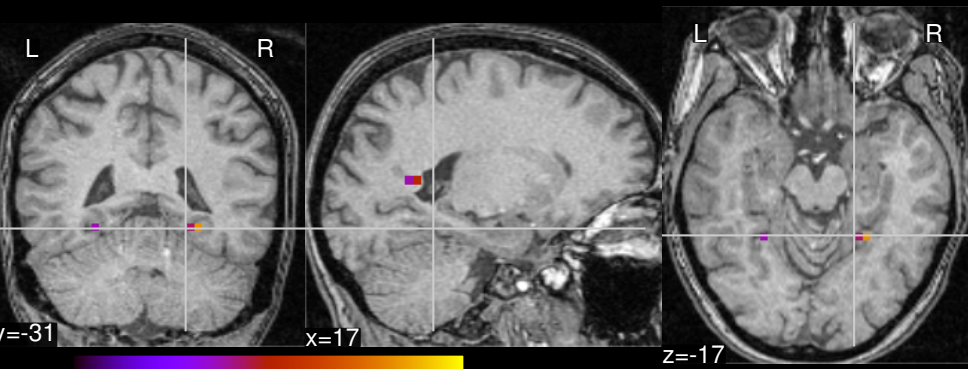
## 4 fMRI: face vs house discrimination [Haxby 2001]

### Univariate F-scores



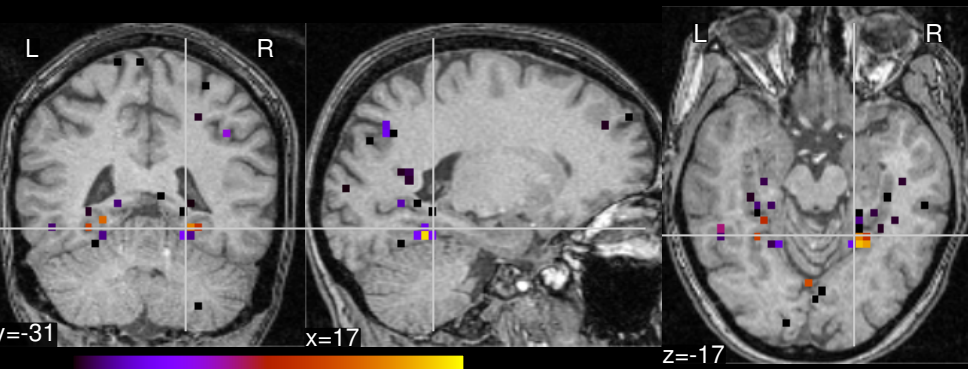
## 4 fMRI: face vs house discrimination [Haxby 2001]

### $l_1$ Logistic



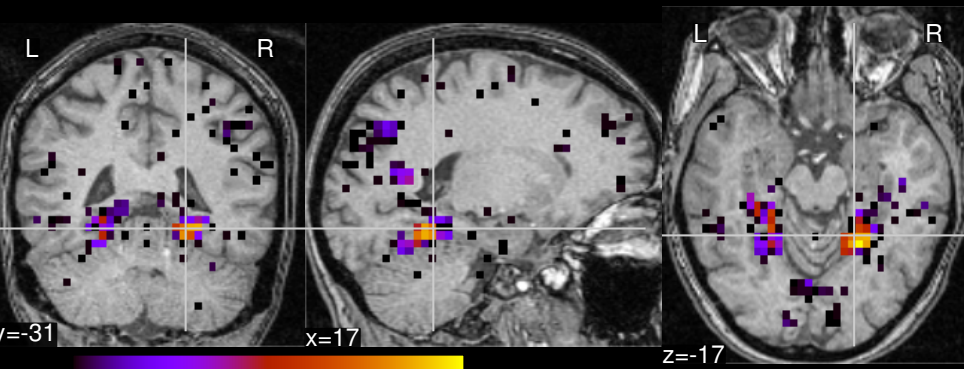
## 4 fMRI: face vs house discrimination [Haxby 2001]

### Randomized $l_1$ Logistic



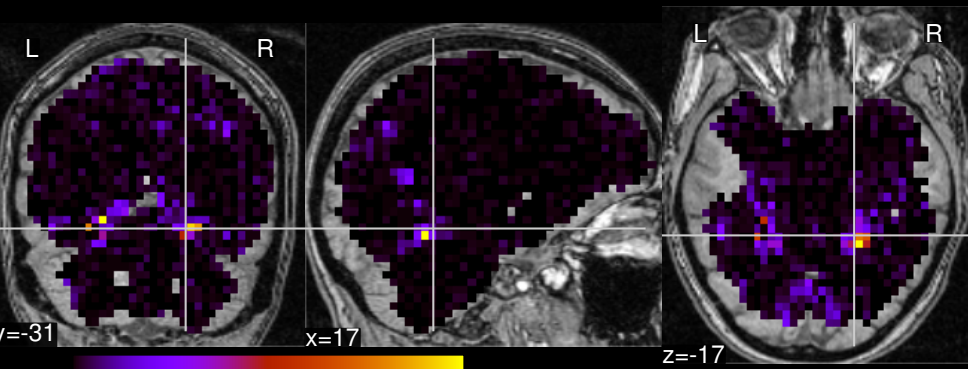
## 4 fMRI: face vs house discrimination [Haxby 2001]

### Randomized Clustered $\ell_1$ Logistic



## 4 fMRI: face vs house discrimination [Haxby 2001]

### F-scores





# 1<sup>st</sup> approach: randomized clustering

**Sparse recovery of patches on spatially-correlated designs**

Ingredients: **Clustering + Randomization**

⇒ Reduced feature set compatible with recovery:  
matches sparsity pattern + recovery conditions

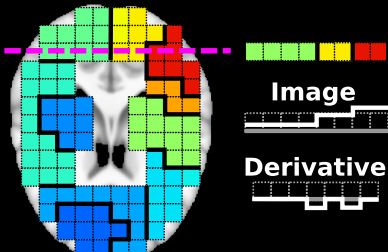
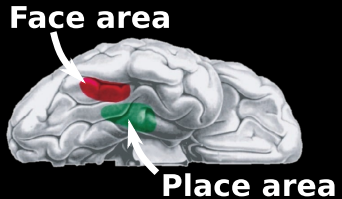
[Varoquaux ICML 2012]

**How to fit in compressive sensing theory?**

## 2<sup>nd</sup> approach: analysis sparsity

$\ell_1$  penalty with an *analysis* operator:  $p(\mathbf{w}) = \ell_1(\mathbf{K}\mathbf{w})$

- Spatial regularization necessary
- Neuroscientists think in terms of brain regions



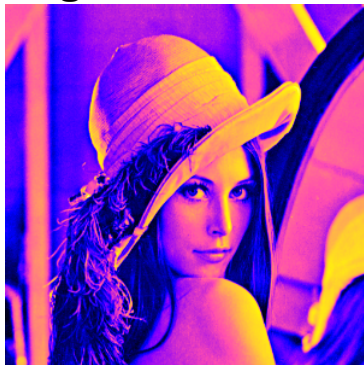
### Total-variation penalization

Impose sparsity on the gradient of the image:

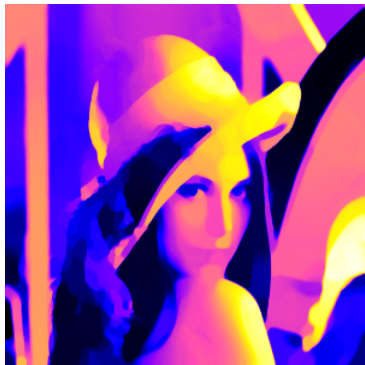
$$p(\mathbf{w}) = \ell_1(\nabla \mathbf{w})$$

In fMRI: [Michel TMI 2011]

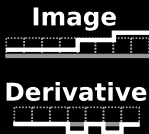
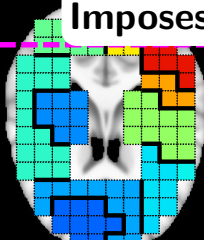
Original



Total-variation



Imposes piecewise-smooth images



Impose sparsity on the gradient of the image:

$$p(\mathbf{w}) = \ell_1(\nabla \mathbf{w})$$

In fMRI: [Michel TMI 2011]

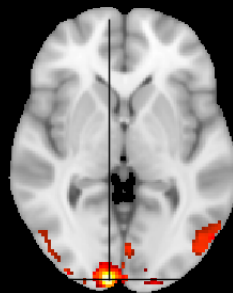
## 4 fMRI decoding with TV

$$\hat{\mathbf{w}} = \underset{\mathbf{w}}{\operatorname{argmin}} l(\mathbf{y} - \mathbf{X}\mathbf{w}) + TV(\mathbf{w})$$

- $l$ : least-square or logistic-regression
- $p$ : TV: isotropic total variation:  $\ell_{21}(\nabla w)$

### Prediction performance:

Feature screening + SVC	0.77
Sparse regression	0.78
<b>Total Variation</b>	<b>0.84</b>
(explained variance)	



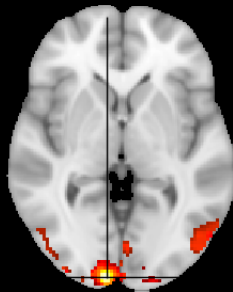
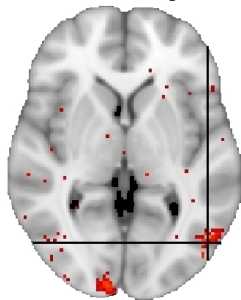
[Michel TMI 2011]

## 4 fMRI decoding with TV

$$\hat{\mathbf{w}} = \underset{\mathbf{w}}{\operatorname{argmin}} l(\mathbf{y} - \mathbf{X}\mathbf{w}) + TV(\mathbf{w})$$

- $l$ : least-square or logistic-regression
- $p$ : TV: isotropic total variation:  $\ell_{21}(\nabla w)$

### Standard analysis



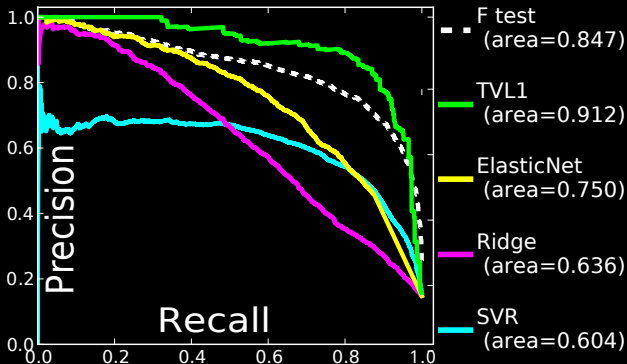
[Michel TMI 2011]

## 4 fMRI decoding with TV- $\ell_1$

$$\hat{\mathbf{w}} = \underset{\mathbf{w}}{\operatorname{argmin}} \|\mathbf{y} - \mathbf{X}\mathbf{w}\| + TV(\mathbf{w}) + \ell_1(\mathbf{w})$$

- Adding  $\ell_1$  = extending analysis operator
- Retrieves sparsity in the original coefficients

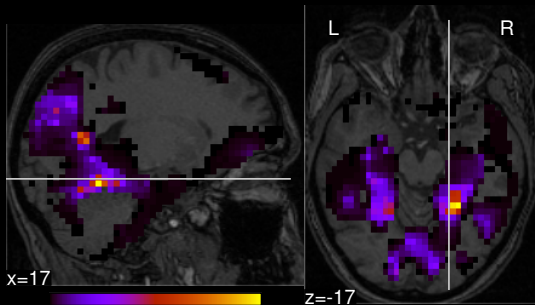
On simulations: sparse recovery precision-recall



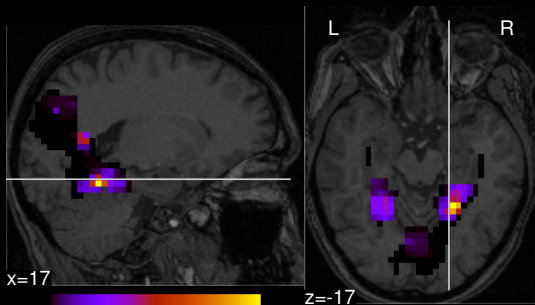
## 4 fMRI decoding with TV- $l_1$ : implementation

Convergence  
matters

Stopping:  
 $\Delta E < 10^{-1}$



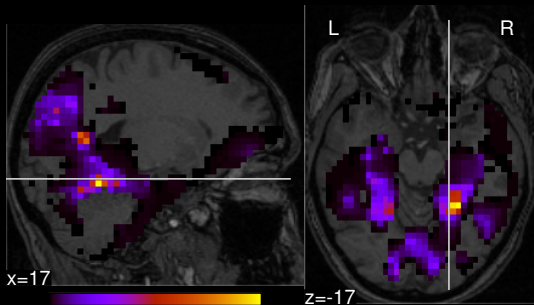
Stopping:  
 $\Delta E < 10^{-3}$



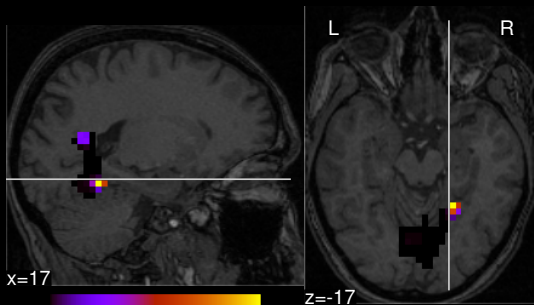
## 4 fMRI decoding with TV- $l_1$ : implementation

Convergence  
matters

Stopping:  
 $\Delta E < 10^{-1}$



Stopping:  
 $\Delta E < 10^{-5}$





## 4 fMRI decoding with TV- $\ell_1$ : implementation

### Optimization algorithms: FISTA

#### ■ FISTA loop for regression:

1. Gradient descent on the datafit term
2. Proximal operator for TV,  
computed with an inner FISTA loop

**Bottleneck:** Gradient descent step costly

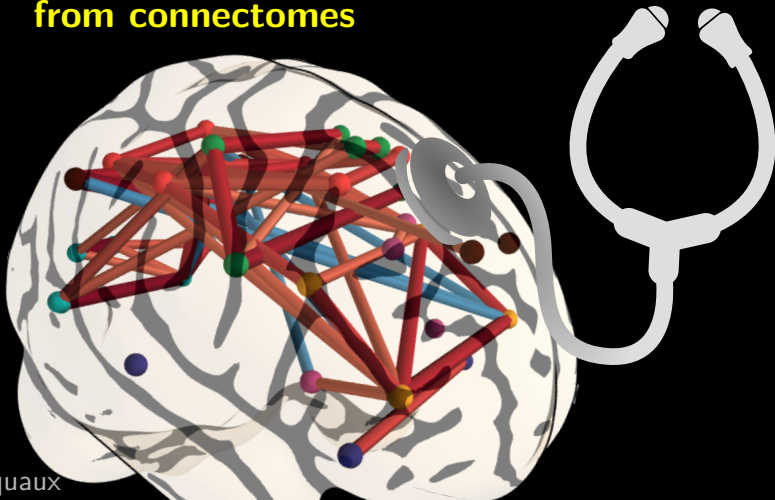
$$\hat{\mathbf{w}} = \underset{\mathbf{w}}{\operatorname{argmin}} \|\mathbf{y} - \mathbf{X}\mathbf{w}\|_2^2 + \ell_1(\mathbf{w})$$

Gradient:  $\mathbf{X}^t \mathbf{X} \mathbf{w}$  with  $\mathbf{X}$  big and dense

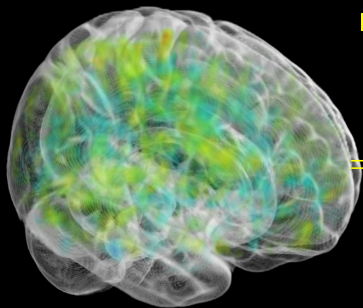
## Take home messages

- Recovery  $\neq$  prediction
- Univariate tests work very well to recover  
Also in genomics [[Haury PLOS One 2011](#)]
- Some form of spatial regularization useful
- Speed matters!  $\mathbf{X}$  : (100 000, 600)

# 5 Learning from spontaneous activity from connectomes



## 5 Resting-state: Spontaneous activity

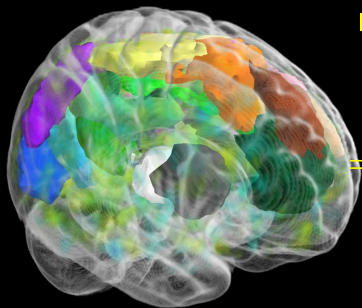


■ In the absence of explicit tasks cognitive circuits are recruited spontaneously

⇒ Meaningful co-fluctuation patterns

**Diagnostic interest  
for disabled patients**

## 5 Resting-state: Spontaneous activity



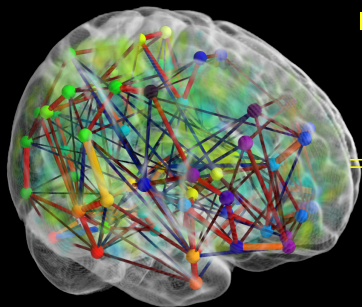
■ In the absence of explicit tasks cognitive circuits are recruited spontaneously

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**Diagnostic interest  
for disabled patients**

1. Learn spatial maps/regions – *Unsupervised learning*

## 5 Resting-state: Spontaneous activity



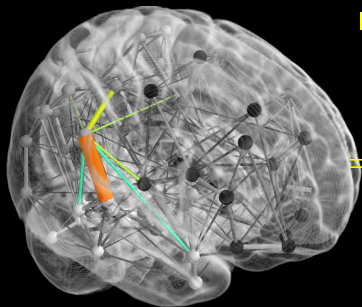
■ In the absence of explicit tasks cognitive circuits are recruited spontaneously

⇒ Meaningful co-fluctuation patterns

**Diagnostic interest  
for disabled patients**

1. Learn spatial maps/regions – *Unsupervised learning*
2. Learn interaction graph – *Unsupervised learning*

## 5 Resting-state: Spontaneous activity



- In the absence of explicit tasks cognitive circuits are recruited spontaneously
- ⇒ Meaningful co-fluctuation patterns

**Diagnostic interest  
for disabled patients**

1. Learn spatial maps/regions – *Unsupervised learning*
2. Learn interaction graph – *Unsupervised learning*
3. Inter-subject/inter-condition prediction –  
*Supervised learning*

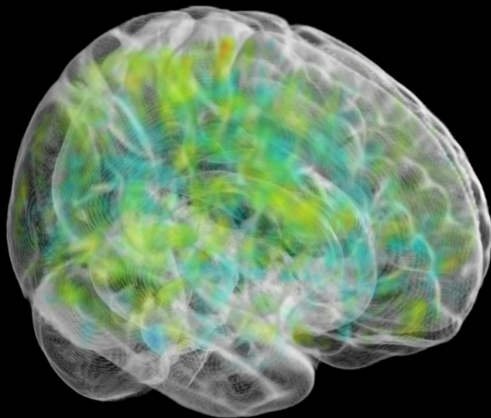
[Varoquaux MICCAI 2010, NIPS 2010, 2011 IPMI, ...]

## 5 Mixture models: linear decompositions

### Working hypothesis:

Observing linear mixtures of networks at rest

Time courses





## 5 Mixture models: linear decompositions

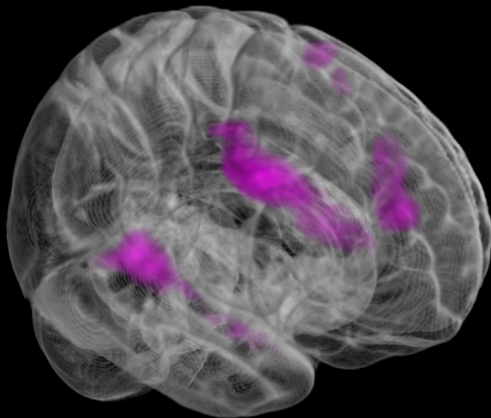
### Working hypothesis:

Observing linear mixtures of networks at rest

Time courses



Language



## 5 Mixture models: linear decompositions

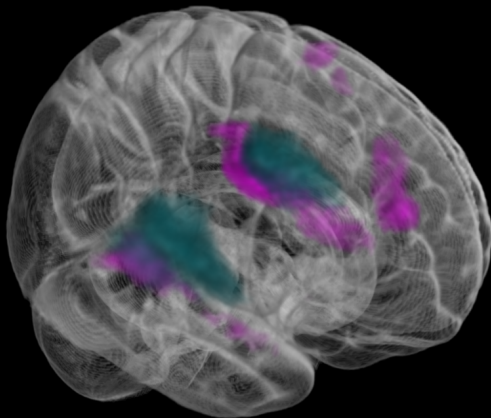
### Working hypothesis:

Observing linear mixtures of networks at rest

Time courses



Audio

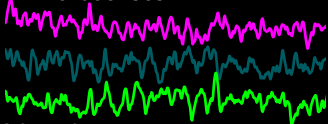


## 5 Mixture models: linear decompositions

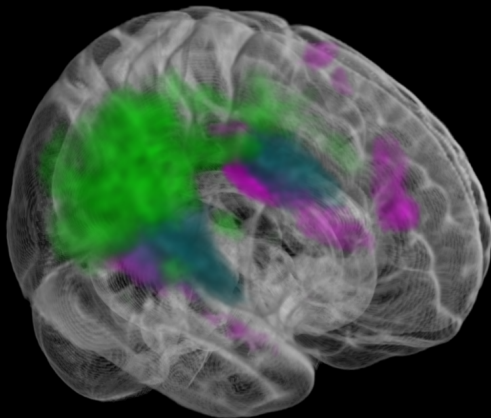
### Working hypothesis:

Observing linear mixtures of networks at rest

Time courses



Visual

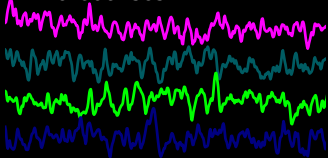


## 5 Mixture models: linear decompositions

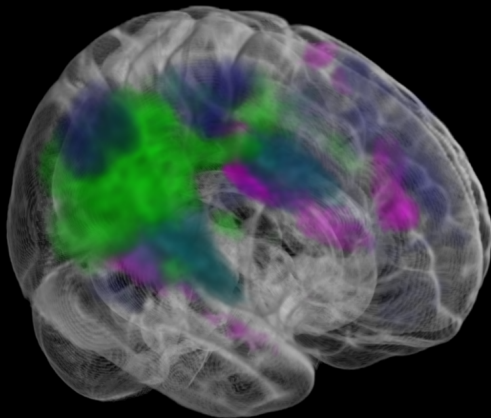
### Working hypothesis:

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Time courses



Dorsal Att.

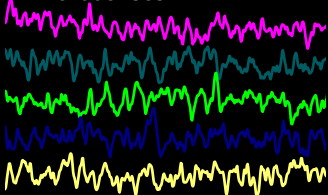


## 5 Mixture models: linear decompositions

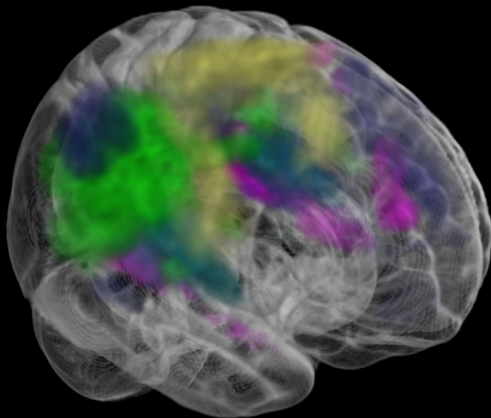
### Working hypothesis:

Observing linear mixtures of networks at rest

Time courses



Motor

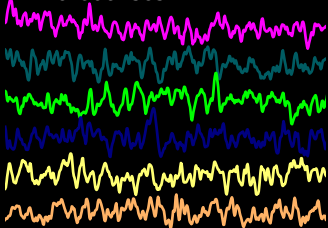


## 5 Mixture models: linear decompositions

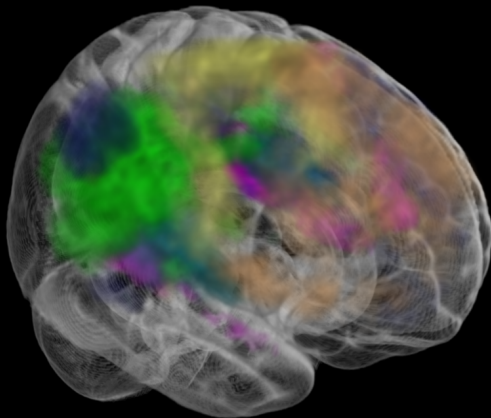
### Working hypothesis:

Observing linear mixtures of networks at rest

Time courses



Saliency

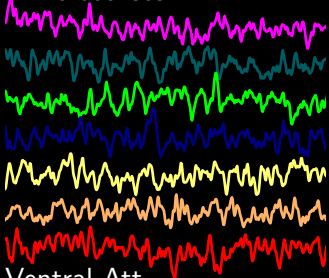


## 5 Mixture models: linear decompositions

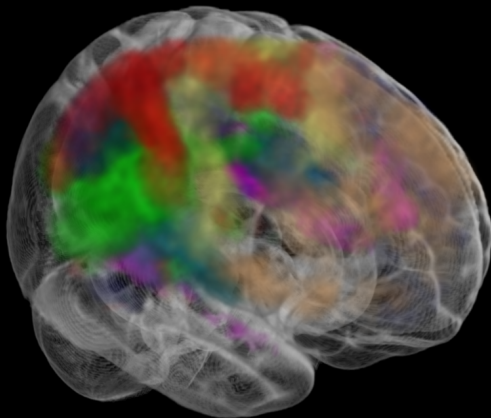
### Working hypothesis:

Observing linear mixtures of networks at rest

Time courses



Ventral Att.

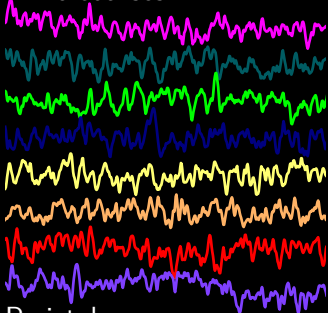


## 5 Mixture models: linear decompositions

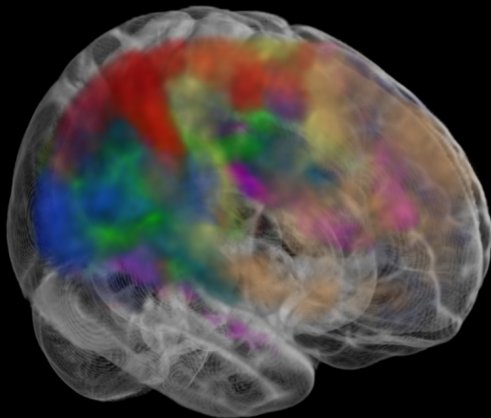
### Working hypothesis:

Observing linear mixtures of networks at rest

Time courses



Parietal



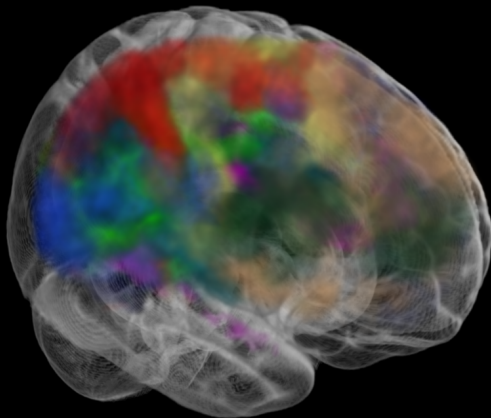
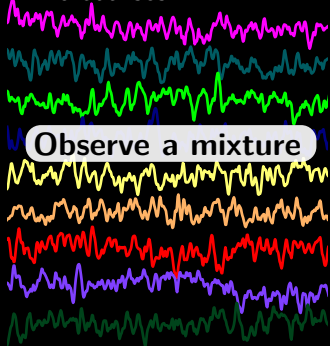


## 5 Mixture models: linear decompositions

### Working hypothesis:

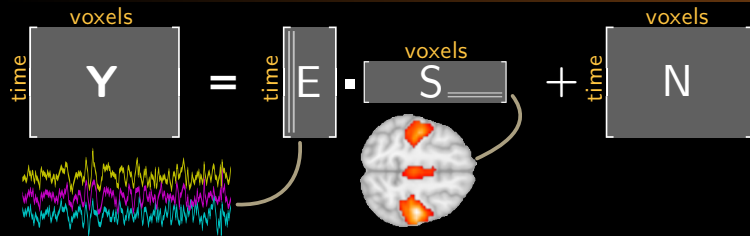
Observing linear mixtures of networks at rest

Time courses



How to unmix networks?

## 5 Segmenting regions from spontaneous activity

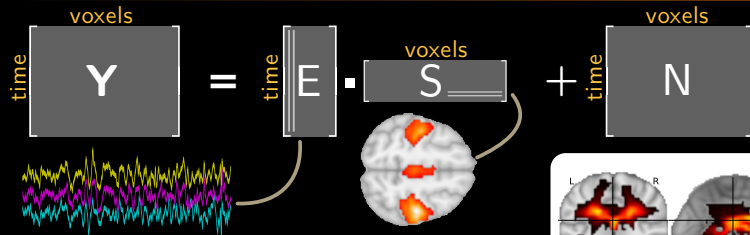


### Linear decomposition model

- spatial maps,  $S$
- residuals,  $N$
- time series,  $E$

### Independent Component Analysis

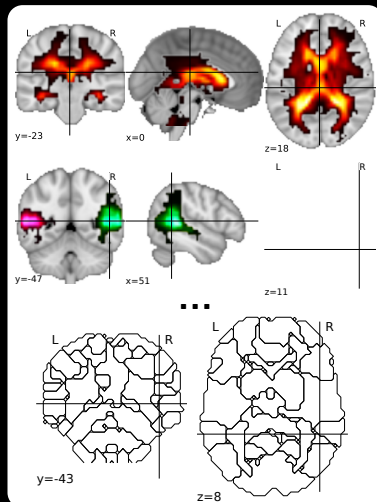
# 5 Segmenting regions from spontaneous activity



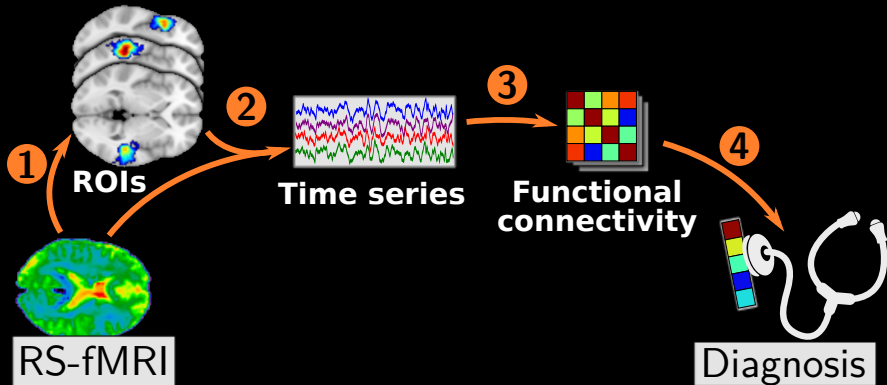
## Linear decomposition model

- spatial maps,  $S$
- residuals,  $N$
- time series,  $E$

**TV- $l_1$  penalty on maps  $S$**



## 5 The connectome classification pipeline



**Preliminary results on Autism**  
**Leave-one-site out cross-validation**  
**⇒ 72% accuracy**

## 6 Beyond equations: software

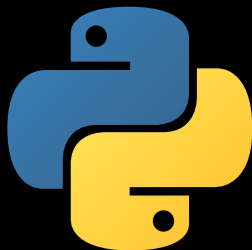


- How to we reach our target audience (neuroscientists)?
- How do we disseminate our ideas?
- How do we facilitate new ideas?



## 6 Python as a scientific environment

- General purpose
- Easy, readable syntax
- Interactive (ipython)
- Great scientific libraries (numpy, scipy, matplotlib...)



## 6 Growing a software stack

- Code lines are costly

- ⇒ Open source + community driven

Need quality and impact

- ⇒ Focus on the general purpose libraries first

**Scikit-learn: machine learning in Python**

<http://scikit-learn.org>

[Pedregosa 2011]

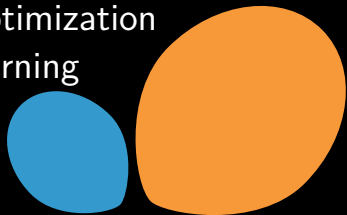
## 6 scikit-learn: machine learning in Python

### Computational performance

	scikit-learn	mlpy	pybrain	pymvpa	mdp	shogun
SVM	<b>5.2</b>	9.47	17.5	11.52	40.48	5.63
LARS	<b>1.17</b>	105.3	-	37.35	-	-
Elastic Net	<b>0.52</b>	73.7	-	1.44	-	-
kNN	0.57	1.41	-	<b>0.56</b>	0.58	1.36
PCA	<b>0.18</b>	-	-	8.93	0.47	0.33
k-Means	1.34	0.79	$\infty$	-	35.75	<b>0.68</b>

- Algorithms rather than low-level optimization  
convex optimization + machine learning

- Avoid memory copies





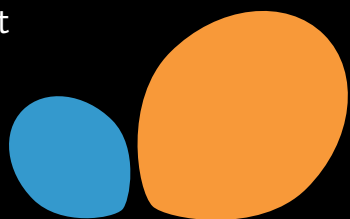
# 6 scikit-learn: machine learning in Python

## Community

- 200 contributors since 2008, 1500 github forks
- 25 contributors in latest release (3 months span)

## Why this success?

- Trendy topic?
- Low barrier of entry
- Friendly and very skilled mailing list
- Credit to people



## 6 Research code $\neq$ software library

### Factor 10 in time investment

- Corner cases in algorithm (numerical stability)
- Multiple platforms and library versions (Blas 😞)
- Documentation
- Making it simpler (and get less educated users)
- User and developer support (  $\sim$  100 mails/day)

**Exhausting,  
but has impact on science and society**

## 6 Research code $\neq$ software library

### Factor 10 in time investment

#### Technical + scientific tradeoffs

---

- Ease of install/ease of use rather than speed
- Focus on “old science”
- Nice publications and theorems are not a recipe for useful code

**Exhausting,  
but has impact on science and society**

## 6 Nilearn: making learning for neuroimaging routine

### Project scope

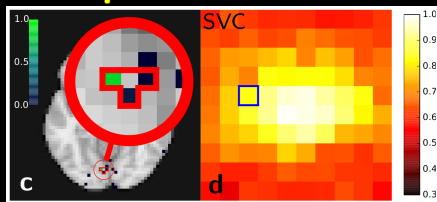
Very preliminary

Machine learning for neuroimaging:  
make using scikit-learn on neuroimaging easy

The target user base is small



### Examples in the docs



Data from Miyawaki 2008

- Run out of the box, downloading **open data**
- Produce a clear figure

Routine, simple, reproduction of papers



# 6 NeuroSynth + NeuroVault: decoding as a service

Neurosynth -- online image decoder - Chromium

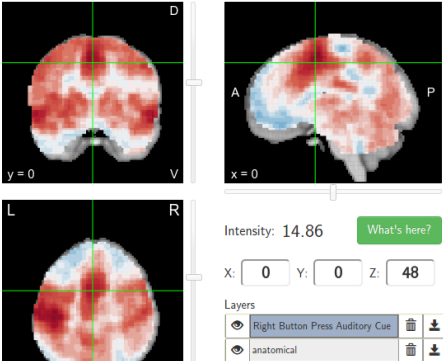
NeuroVault: a new ho x Neurosynth -- online i x

neurosynth.org/decode/?neurovault=394

Neurosynth.org (beta) Home Features Studies Locations Decoder Code FAQs

## Decoding results

Map Plot



Intensity: 14.86 [What's here?](#)

X: 0 Y: 0 Z: 48

Layers

<input checked="" type="checkbox"/>	Right Button Press Auditory Cue	<input type="checkbox"/>	<input type="checkbox"/>
<input checked="" type="checkbox"/>	anatomical	<input type="checkbox"/>	<input type="checkbox"/>

### Feature loadings

To compare the decoded image against a term, click on an arrow below.

Show 10 entries

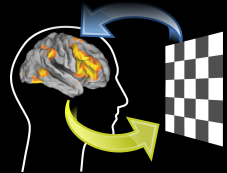
Search:

feature	corr
<input type="checkbox"/> auditory	0.535
<input type="checkbox"/> sounds	0.437
<input type="checkbox"/> listening	0.437
<input type="checkbox"/> sensorimotor	0.387
<input type="checkbox"/> somatosensory	0.383
<input type="checkbox"/> execution	0.348
<input type="checkbox"/> music	0.346
<input type="checkbox"/> speech production	0.344
<input type="checkbox"/> hand	0.335

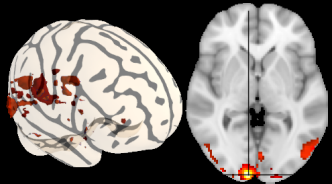
# Machine learning for brain imaging

# Statistical learning to study brain function

- Learning problems, but not only about prediction error



- Spatial regularization for linear models  
Total variation + randomization



- Validation is very hard  
All model are wrongs, and data is scarce

- Speed and parameter selection matter  
Users will not adapt

**Positions available**

# Bibliography

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